



Short Communication Volume 4 Issue 1 – February 2017 DOI: 10.19080/ADOH.2017.04.555627 **Adv Dent & Oral Health**

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Extracted Tooth: Can it be A Bone Graft Substitute?



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Submission: February 01, 2016; Published: February 28, 2017

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Abstract

This article introduces the use of Demineralized Dentin Matrix (DDM) scaffold, which are fabricated from the patient's own extracted tooth to repair the alveolar bone defect under the view point of clinical implant dentistry. DDM is natural collagen based scaffold with similar organic and inorganic component of autogenous bone. The possibilities of DDM as bone graft substitute are compared to well known demineralized bone matrix (DBM) which has a little limitations. Based on *in vitro* and *in vivo* studies on DDM, clinical applications of DDM as three dimensional scaffolds for alveolar bone regeneration have shown predictability as well as possibilities of future advancement to the carrier of growth factors and stem cells.

Keywords: Demineralized dentin matrix, Demineralized bone matrix

Abbreviation: DDM: Demineralized Dentin Matrix; DBM: Demineralized Bone Matrix

Introduction

Dentin

Autogenous bone graft has been generally carried out for the repair of alveolar bone defect as a gold standard. To avoid and overcome the disadvantages of not only donor site morbidity and complications but also the limited supply, the development for bone substitutes as an alternative of autogenous bone have begun. And various artificial materials including ceramic material, synthetic biological material nano-material have been developed.

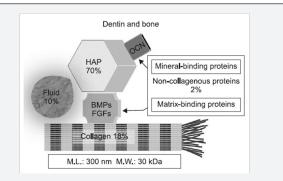


Figure 1: Diagram of common components in dentin and bone. (HAP: hydroxyapatite, OCN: osteocalcin, BMP: bone morphogenetic protein, FGFs: fibroblast growth factors).

One of the alternatives recently developed is dentin, which has been discarded after extraction. Because the structure and composition of dentin are similar to that of bone, consisting of collagen (20%), hydroxyapatite (70%), and body fluid (10%) in weight (Figure 1) [1-5]. Bone inducing molecules, such as bone morphogenetic proteins (BMPs), was also identified from rat, rabbit and bovine derived bone and dentin [6,7]. Moreover, BMPs derived from human dentin induced new bone formation [7,8].

Apart from these molecules, dentin collagen is the most highly insoluble matrix due to its cross-linking [9], with osteoinductive growth factors that provide an appropriate environment for osteoinduction [8,10]. Dentin matrix-derived BMP is not exactly same as bone matrix-derived BMP, but they are very similar. In other words, two types of BMP exhibit the same action in the body [111]

The collagenous dentin matrix is a repository of bone morphogenetic proteins (BMPs), transforming growth factor- β (TGF- β), insulin-like growth factor (IGF), and basic fibroblast growth factor (bFGF). In addition, the concentration of TGF- β , insulin growth factor-I (IGF-I), insulin growth factor-II (IGF-II) fibroblast growth factor (aFGF, bFGF), and platelet derived growth factor (PDGF) were detected in human DDM. However,

the concentrations of these growth factors in dentin were lower, compared to bone [10,12].

Several non-collagenous proteins such as osteocalcin (OCN) and osteopontin (OPN) are common in dentin and bone, while dentin phosphoprotein (DPP) (so-called phosphophoryn) is a specific non-collagenous protein in dentin (Figure 1). DSP is a dentin-specific non-collagenous protein involved in the calcification of dentin and suggested that dentin has high affinity for and marked osteoconductive effect on the jaw bone [5,13-16].

Clinically, it also can be defined as reprocessed natural collagenous scaffold with endogenous growth factors among acid-soluble, acid-insoluble, heat-denatured gelatin and pepsin digested atelocollagen (Table 1) [5].

Table 1: Comparison of collagenous materials. (RGD; Arginylglycylaspartic acid, DDM: Demineralized Dentin Matrix, DBM: Demineralized Bone Matrix).

	Structure	Solubility	RGD	Specific Protein
DDM	Dentinal tubes	Acid- insoluble	+	Phosphophoryn DMP-1
DBM	Cell lacunae capillary spaces marrow spaces	Acid- insoluble	+	Osteocalcin DMP-1
Atelocollagen	Fiber	Acid- soluble pepsin- digested	+	70
Gelatin	Plate-like	Heat- denatured	-	

Demineralized bone matrix (DBM) vs demineralized dentin matrix (DDM)

The idea of DDM is basically comes from DBM. DBM is prepared by demineralization of allograft bone [17]. It results in the elimination of the major part of the mineral phase and the immunogenic components of bone [18,19].

It has been speculated that the osteoinductive growth factors contained in the dentin matrix are more easily accessed and unshielded once the mineral phase of the dentin has been removed by demineralization [20]. Demineralization with 0.6N HCL results in the elimination of the major part of the mineral phase retaining a very low fraction of mineral in dentin (10-30% approx.) and the immunogenic components, but retains Type I collagen that provides an osteoconductive scaffold and a soluble protein fraction comprising several GFs, BMPs among them [21-23]. As a result, DDM increased their osteoinductivity and decreased their antigenicity after demineralization [17-20].

DBM by itself is presented in the form of a powder, but is usually mixed with other suitable materials (e.g. hyaluronan, poloxamer) to form a paste that can be easily molded at the bone defect [19,21]. DDM powder is prepared by crushing the dentin into $300\text{-}800\mu\text{m}$ sized particles. Each DDM powder possesses

dentinal tubule-derived micropore spaces (diameter: 0.8-1.0µm, approximately 50,000 tubes/mm²). This pore size is too small for the infiltration and ingrowth of cells. Once dentin is demineralized, the dentinal tubule would become wider and serve as a channel for releasing essential proteins, which may promote growth and differentiation of osteoblasts. Enlarged dentinal tubules and loosened collagen by demineralization enhanced surface microroughness or micro-texture to help easy releasing of signaling factors and remodeling [1,18,22]. For an average follow-up of at least 5 years, DDM powder showed that cortico-cancellous bone had been maintained successfully after functional loading, which illustrates the remodeling capacity of DDM powder [23].

DDM block, fabricated from root dentin, is a biomimetic of cortical bone that exhibits slow creeping substitution properties with 3 to 5lm innate micropores (dentinal tubules) and 0.2 to 0.3mm macropores. DDM block is well incorporated and remodeled into cortico-cancellous bone with dental implant after average 44 months of follow-up [24,25].

DBM can be supplemented with additional growth factors in an attempt to boost their regenerative capacity. DBM has been mainly loaded with BMPs and particularly, with BMP-2 for bone tissue engineering [26,27]. DDM can also be supplemented with rhBMP-2 to enhance bone forming capacity by its endogenous and exogenous growth factors [28-30].

Conclusion

Human DDM, prepared by demineralization process of extracted teeth either orthodontic or pathologic origin, can be defined as acid-insoluble, cross-linked collagen with natural growth factors, absorbable, and elastic material with original dentin structures. Reprocessed dentin scaffolds represent probably the most advanced scaffolds available because it has not only the complex composition, but also the structure of the native tissues. This cannot be achieved with the scaffolds prepared from synthesis and tissue engineering such as those presented before.

Acknowledgment

This study was supported in part by a grant from the Korean Health Technology R&D Project, Ministry of Health & Welfare, Republic of Korea (HI15C3136).

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