

Marginal Fit Comparison of Hot Isostatic Pressed and Non-Hot Isostatic Pressed Zirconia Copings with Three Different Marginal Finish Lines Fabricated with Two Different CAD-CAM Systems



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Abstract

Purpose: The aim of this study was to compare the marginal fit of hot isostatic pressed (HIP) and non-hot isostatic pressed (NON-HIP) zirconia copings with three different marginal finish lines fabricated with two different CAD-CAM systems.

Methods: 60pcs. Stainless steel specimens, which are 6 mm crown length 2mm finish lines width and 60 degree axial wall inclination angle were prepared. These specimens were prepared 3 different marginal finish lines as shoulder finish line (SHO), chamfer finish line (CHA), bevel finish line (BEV). 30 NON-HIP zirconia copings with Cerec in Lab System, and 30 HIP zirconia copings with DCS Precedent System were fabricated with shoulder, chamfer and bevel finish lines as 10 each groups. Totally 60 zirconia coping specimens were randomly assigned in 6 experimental groups (n=10).

Results: Marginal gap measurements were performed using a stereomicroscope with x150 magnification. The average measurement values were obtained as follows, respectively: Group SHO/HIP (35,8±13,5µm) < Group CHA/HIP (44,3±13,3µm) < Group BEV/HIP (55,7±27,6µm) < Group CHA/NHIP (60,2±24,4µm) < Group SHO/NHIP (85,6±25,6µm) < Group BEV/NHIP (86,6±35,8µm). Statistically significant difference was found between HIP and NON-HIP groups (p<0.001), and between groups with different finish line (p<0.001).

Conclusion: The marginal gap of zirconium frameworks has been affected by the type of finish line and different CAD-CAM systems.

Keywords: Cad-cam; Marginal adaptation; Zirconium oxide

Abbreviations: CAD: Computer-Aided Design; CAM: Computer Aided Manufacturing; HIP: Hot Isostatic Pressed; NON-HIP: Non-Hot Isostatic Pressed; SHO: Shoulder; CHA: Chamfer; BEV: Bevel

Introduction

Owing to their superior aesthetic and functional properties fixed ceramic restorations became an integral part of the daily dental practice. However, it is well known that porcelain fused to metal restorations can cause metal-ion discoloration, corrosion, prevention of the light transmission and allergic reactions. [1-7] Therefore, aesthetically superior metal free porcelain systems have been developed and gained their popularity in the last decade with the use of all-ceramic framework materials such as lithium disilicate, aluminum oxide and zirconium oxide [8-10]. Apart from their mechanical strength other important issues related to physical properties of ceramic restorations are their biocompatibility and marginal adaptation. Marginal adaptation in fixed restorations is

thought to be one of the most decisive factors in long-term success of the prosthetic rehabilitation [11]. Marginal gaps around fixed restorations might result in plaque accumulation, micro leakage, decrease in gingival curricular fluid, caries formation and bone loss associated with periodontal destruction. [12,13]. A literature survey revealed that, up to 120µm gap around a fixed restoration could be accepted as within clinically acceptable limits [11,14-17]. In the last two decades the use of computer-aided design (CAD) and computer aided manufacturing (CAM) technologies allowed manufacturing of highly resistant ceramic materials which are serving satisfactory results in terms of aesthetics and durability [18,19]. There are two different types of CAD/CAM systems. The

first type is the use of fully sintered (hot isostatically pressed) dense blocks. The future of this system makes direct machining by using grinding machine with high strength. The other type is the use of partially sintered blocks (non-hot isostatically pressed). This system need post-sintering to obtain a final product with sufficient strength. Currently different zirconium oxide ceramic systems such as Cercon (Dentsply), Precident DCS (DCS Dental AG), Lava (3M ESPE), Procera All Zirkon (Nobel Biocare) and Cerec inlab (Cerec inLab® MC XL, Sirona Dental Systems, Bensheim, Germany) were also developed [20-22]. The aim of this in-vitro study was to compare the marginal fit of hot isostatic pressed (HIP) and non-hot isostatic pressed (NON-HIP) zirconia copings with 3 different marginal finish lines fabricated with two different CAD-CAM systems. It was hypothesized that the frameworks fabricated with shoulder marginal finish line and by DCS Precident® CAD/CAM system would be associated with less marginal gap.

Materials and Methods

In order to simulate prepared teeth, 60 stainless steel specimens were fabricated in CNC lathe (Samsung PL 15A/300, Ankara, Turkey). Specimens had a length of 6mm, marginal width of 1.2mm and preparation angle of 6 degrees. Three finish line designs were prepared among 3 experimental groups: shoulder (SHO), chamfer (CHA) and bevel (BEV) (n=20). These 3 experimental groups were divided to two sub-groups as HIP and NON-HIP according to the zirconium core material type and production methods (SHO/HIP, SHO/NHIP, CHA/HIP, CHA/NHIP, BEV/HIP and BEV/NHIP). HIP zirconia specimens were produced by DCS Precident® CAD-CAM system and NON- HIP zirconia specimens were produced by Cerec in lab® CAD-CAM system (Figure 1).

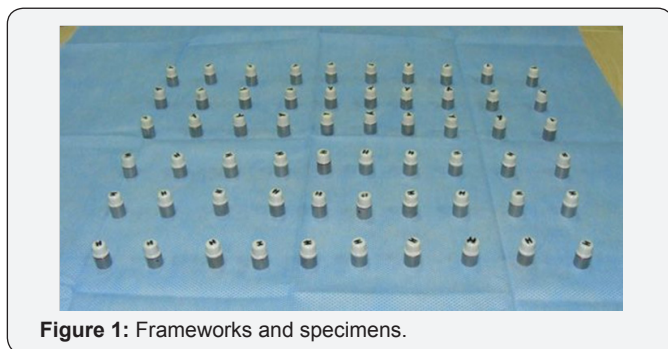


Figure 1: Frameworks and specimens.

Preparation of frameworks with Cerec in Lab® system

For the preparation of NON-HIP zirconium frameworks with Cerec in Lab® system, (Cerec in Lab® MC XL, Serena Dental Systems, Blenheim, Germany) surfaces of stainless steel specimens were coated with the titanium oxide powder (Powder Cerec, Vita, Germany). Images of specimens coated titanium oxide were transferred and designed via digital image device of Cerec in Lab® system. Marginal limits of restorations on digital impressions were determined and restorations within the marginal limits were composed in digital platform. Thicknesses of frameworks were adjusted as 0.5 mm on Cerec in Lab® software program. Ceramic blocks (Vita In-Ceram YZ Zirconia, VITA Zahnfabrik) were placed

to the milling section of the device. After dimensional values of specimens were transferred to milling section of the device milling process by calibrating has started. After milling, the frameworks have sintered to achieve the final density and maximum strength of the material.

Preparation of frameworks with DCS precedent system

HIP zirconia frameworks were fabricated from fully-sintered DC-zirconia blocks by using DCS Precident® CAD-CAM systems (DCS-Precident®, DCS Dental AG and CH-Allschwil, Germany). Surfaces of specimens were scanned with laser scanner and configuration of the frameworks was created digitally. The milling process was completed in approximately 3 hours.

Marginal Gap Measurements

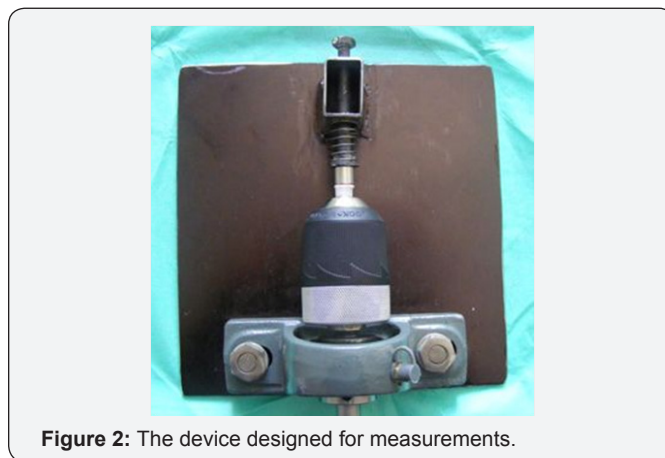


Figure 2: The device designed for measurements.

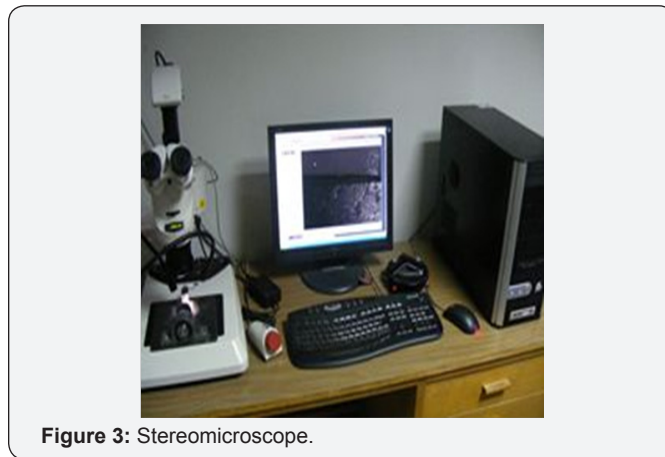


Figure 3: Stereomicroscope.

These measurements were performed at 32 different points across the entire circumference of each framework. A special device was designed to keep constant forces and standard positioning of the specimens under the microscope (Figure 2). Measurements were conducted by a stereomicroscope (Leica MZ 16 FA, Wetzlar, Germany) via a special software (Leica Image Manager IM 1000V 4.0 R117, Wetzlar, Germany) with a x250 magnification integrated with a digital camera (Leica DFC 420, Wetzlar, Germany) at General Directorate of Mineral Research and Exploration Department of Mineralogy and Petrography Laboratory (Figure 3). Examination of marginal fit of frameworks was performed under a stereomicroscope

with x150 magnification. The images of all frameworks were taken with the same magnification and standard position under stereomicroscope. Prior to measurements of the marginal gaps in order to easily view the marginal zone, the marginal edges of specimens were painted by a red marking pencil with an angle of 45 °degree (Figure 4). The photographs were taken at 8 points. 32 measurement values were taken from each specimen with 4 measurement values on each selected point (Figure 5). 960 measurement values for the each group were obtained. In case the guide point resembled a non-uniform marginal discrepancy or cracked area was observed during the analysis of the photos for measurement a different point was chosen at the same photo for the measurement in order to eliminate measurements without representative marginal discrepancies.

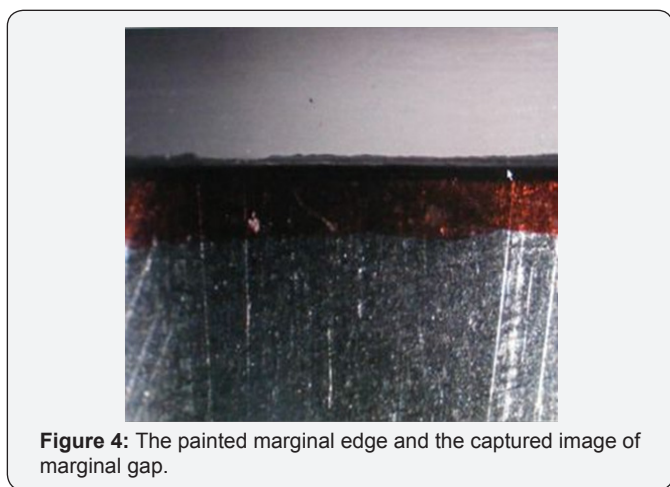


Figure 4: The painted marginal edge and the captured image of marginal gap.

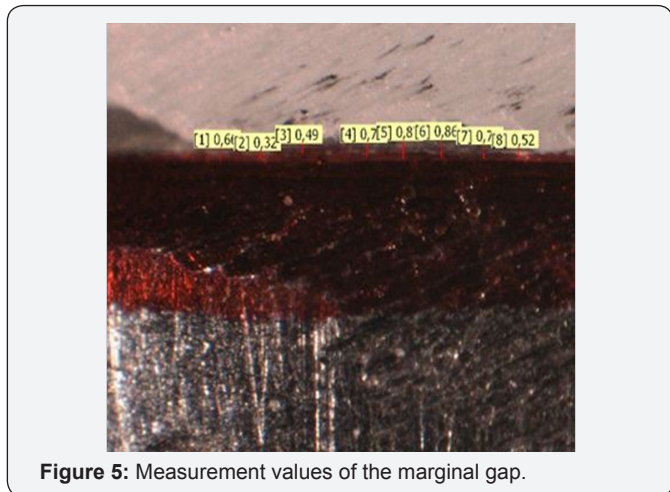


Figure 5: Measurement values of the marginal gap.

Statistical analysis

SPSS 15.0 (SPSS Inc. USA) software was used for the statistical analysis. For the identification of data, mean, median, minimum-maximum and standard deviation values were calculated. Compliance of continuous variables with normal distribution was analyzed by using the Kolmogorov-Smirnov test. Kruskal-Wallis test was used in comparison of multiple groups. Comparison of main groups was made by Mann-Whitney U test with Bonferroni correction. Statistically $p < 0.05$ was considered as significant.

Results

Measurements, means, standard deviation, median, minimum- maximum values among NON-HIP groups (SHO/NHIP, CHA/NHIP, BEV/NHIP) and HIP (SHO/HIP, CHA/HIP, BEV/HIP) groups were shown in micrometer (μm) in Table 1-2. Marginal gap values of different finish lines were shown in Table 3. The comparison of (SHO/NHIP) & (SHO/HIP), (CHA/NHIP) & (CHA/HIP), (BEV/NHIP) & (BEV/HIP) groups are shown in Figure 6-8. Marginal gap values of six experimental groups were listed from smaller to larger as follows: SHO/HIP $35,8 \pm 13,5\mu\text{m}$ < CHA/HIP $44,3 \pm 13,3\mu\text{m}$ < BEV/HIP $55,7 \pm 27,6\mu\text{m}$ < CHA/NHIP $60,2 \pm 24,4\mu\text{m}$ < SHO/NHIP $85,6 \pm 25,6\mu\text{m}$ < BEV/NHIP $86,6 \pm 35,8\mu\text{m}$. The comparison between the same kinds of finish lines prepared with different systems revealed statistically significant differences ($p < 0,001$) (Table 4).

Table 1: Marginal gap values obtained in NON-HIP groups (μm).

Sub Groups	Specimens	Mean	Standard Deviation	Median	Min.	Max.
SHO/NHIP	1	72,08	29,00	69,00	25,5	125,5
	2	63,66	21,93	56,25	31,5	121,5
	3	87,75	16,74	89,25	46,5	117,5
	4	69,50	16,20	73,50	36	96
	5	95,83	15,72	99,75	66	118
	6	90,91	23,17	90,25	57,5	165
	7	78,60	27,96	73,50	36	132,5
	8	111,13	13,97	114	78	132
	9	83,88	22,27	78,75	43,5	129
	10	102,75	22,93	114,75	57	136,5
CHA/NHIP	1	77,20	24,44	73,50	45,5	130,5
	2	58,86	17,62	57,75	28,5	100,5
	3	39,91	7,81	39	27	55,5
	4	66,43	28,41	57,75	25,5	121,5
	5	61,21	25,13	57	25,5	120,5
	6	67,01	28,13	68,50	25,5	121,5
	7	49,23	16,31	48	25,5	88,5
	8	53,98	18,41	57	16,5	88,5
	9	57,03	24,91	57	25,5	108
	10	71,21	24,80	68	33	117
BEV/NHIP	1	97,51	15,58	100	65	118,5
	2	74,55	23,89	73,50	27	130,5
	3	54,66	23,97	52,50	25,5	112,5
	4	82,71	39,11	73,50	26	165
	5	77,46	29,05	73,50	34,5	157
	6	70,18	28,95	65,25	31,5	156
	7	118,53	27,74	126,5	58,5	157
	8	97,70	42,86	87	34	177
	9	111,68	33,73	118,25	48	169,5
	10	81,15	36,50	69	33	156

Table 2: Marginal gap values obtained in HIP groups (μm).

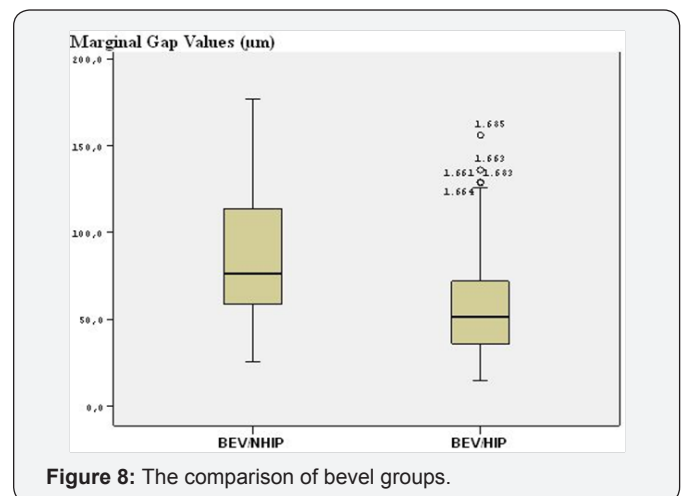
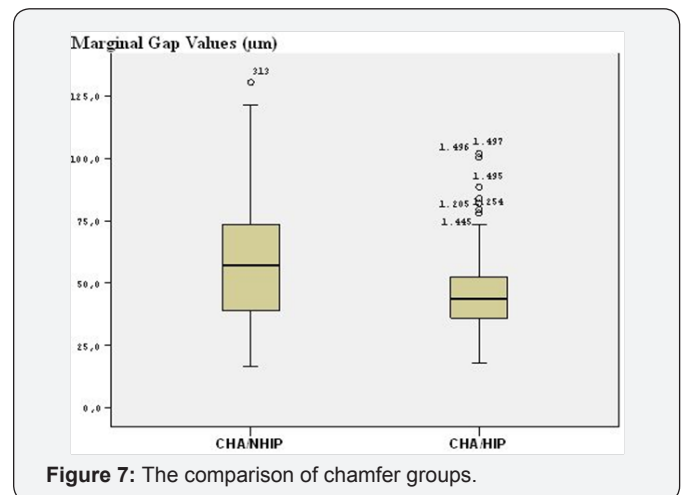
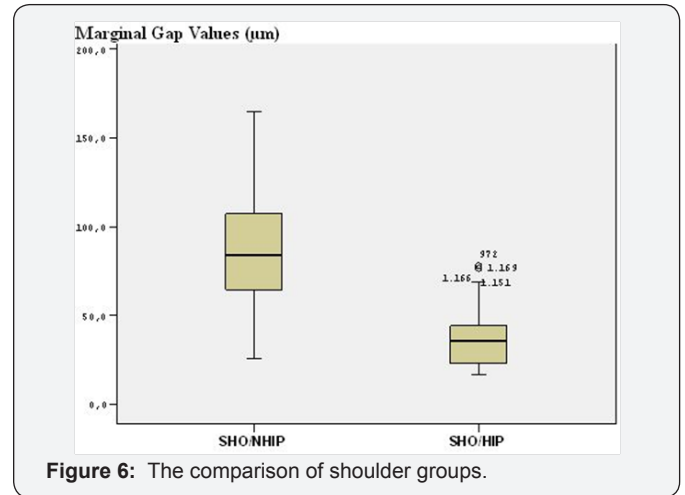
Sub Groups	Specimens	Mean	Standard Deviation	Median	Min.	Max.
SHO/HIP	1	37,66	10,48	36,25	16,5	61,5
	2	24,98	7,73	22,50	16,5	40,5
	3	33,73	15,28	34,50	16,5	78
	4	33,68	10,56	36	16,5	57
	5	30,21	12,85	25	16,5	61,5
	6	31,83	12,55	28,50	16,5	66
	7	41,83	10,40	73,50	36	132,5
	8	42,85	12,10	40,50	21,5	65
	9	48,35	14,81	43,25	28	78
	10	33,38	12,00	32,25	16,5	52,5
CHA/HIP	1	53,15	12,68	51,75	34,5	78
	2	40,61	13,02	39	25,5	78
	3	43,95	6,52	43,5	34,5	58,5
	4	41,61	9,53	42	25,5	60
	5	43,83	14,53	43,50	19,5	67,5
	6	43,46	13,33	40,5	25,5	78
	7	37,30	8,50	39	25,5	60
	8	38,65	10,51	39	18	54
	9	44,55	11,63	40,5	27	78
	10	55,96	18,62	48	34,5	102
BEV/HIP	1	50,51	13,37	51	28,5	78
	2	60,15	27,94	66,75	16,5	99
	3	67,41	28,80	62,25	32	114
	4	41,56	17,40	39,5	15	78
	5	48,31	25,92	49,5	16,5	93
	6	71,23	40,13	67,5	16,5	136
	7	63,58	37,71	59,25	16,5	156
	8	45,36	19,14	48,25	16,5	78
	9	48,60	17,17	45	16,5	78
	10	60,81	20,80	60,25	25,5	112,5

Table 3: Marginal gap values of different finish lines (μm).

Main Groups	Subgroups	Mean \pm Standard Deviation (μm)
NON-HIP	SHOULDER	85,6 \pm 25,6
	CHAMFER	60,2 \pm 24,4
	BEVEL	86,6 \pm 35,8
HIP	SHOULDER	35,8 \pm 13,5
	CHAMFER	44,3 \pm 13,3
	BEVEL	55,7 \pm 27,5

Table 4: The comparison of the same kind of finish lines of two main groups.

Main Groups	P
SHO/NHIP > SHO/HIP	<0,001
CHA/NHIP > CHA/HIP	<0,001
BEV/NHIP > BEV/HIP	<0,001



Discussion

The purpose of this in-vitro study was to compare the marginal fit of hot isostatic pressed (HIP) and non-hot isostatic pressed (NON-HIP) zirconia copings with 3 different marginal finish lines fabricated with two different CAD-CAM systems. In the current study, 60 stainless steel specimens were fabricated for the simulation of the prepared teeth. Due to the difficulties of ensuring a standard preparation in natural teeth, stainless steel specimens were preferred instead of natural tooth. To ensure standardization, metal or resin dies were used in several studies evaluating the marginal adaptation [23,24]. Three finish line design were prepared; shoulder preparation (SHO), chamfer preparation (CHA) and bevel preparation (BEV) (n=20). Each finish line was fabricated twenty items according to the manufacturer's recommendations. 3 experimental groups were divided to two sub-groups includes HIP and NON-HIP based on the zirconium core material type and production method (SHO/HIP, SHO/NHIP, CHA/HIP, CHA/NHIP, BEV/HIP and BEV/NHIP). HIP zirconia specimens were produced by DCS Precedent CAD-CAM system and NON- HIP zirconia specimens were produced by Cerec in Lab CAD-CAM system. According to the results of study the marginal discrepancy of NON-HIP zirconium frameworks was measured as 85, 6µm in the shoulder finish line group (SHO/NHIP), 60, 2µm in chamfer finish line group (CHA/NHIP) and 86, 6µm in bevel finish line group (BEV/NHIP). The marginal discrepancy of HIP zirconium frameworks was measured as 35, 8µm in the shoulder finish line group (SHO/HIP), 44, 3µm in chamfer finish line group (CHA/HIP) and 55, 7µm in bevel finish line group (BEV/HIP). The lowest marginal discrepancy amount was found on SHO / HIP group. Based on these findings, the shoulder finish line and hot isostatic pressed group provided better results, thus supporting the hypothesis of the present study. Considering similar studies in the literature, marginal discrepancy values could vary between 28-160µm [25-27]. However, according to some authors, 200µm is the adequate marginal discrepancy value for an acceptable restoration [28,29]. Coli & Karlsson [30] reported that the mean value of the marginal gap measurements between the frameworks and the master models was a range of 0 to 115µm and therefore these values were clinically acceptable. Tinschert et al. [31] showed that the measurements of the marginal fit of the FPDs with DC-Zirkon framework exhibited mean marginal discrepancies in a range between 60.5 and 74.0µm. Bindl et al. [32] reported that marginal gap width were DCS (110 +/- 79µm) and Cerec in Lab (114 +/- 58µm) in their study on 72 specimens. Komine et al. [33] fabricated forty-eight standardized partially sintered ZrO₂ ceramic four-unit FPD frameworks using three different CAD/CAM systems (Cercon Smart Ceramics (group CE), Vita YZ/Cerec In-Lab (group YZ/CL) and Xidex (group XA)) Geometrical means of the marginal discrepancies were evaluated and found a gap amount of 120.0 micro/88.0 micro for the curved/straight design of CE group, 96.8micro/86.5micro for YZ/CL group and 147.3micro/113.4micro for the XA group. They have reported significant differences between straight and curved

designs for groups CE (p=0.001) and XA (p=0.003). The marginal discrepancies were significantly smaller in group YZ/CL than in group XA for the curved design and the marginal discrepancies in group YZ/CL were also significantly smaller than those in group CE. These results are consistent with the results of the study considering the difference between shoulder and bevel groups. McLean & von Fraunhofer [34] proposed that a restoration would be successful if marginal gaps and cement thickness of less than 120µm could be achieved. Among zirconium frameworks fabricated in the current study, the lowest marginal gap values were found in the SHO / HIP group (35, 8µm) whereas the highest marginal gap values were observed in the BEV / NHIP group (86, 6µm). The entire values were found clinically within acceptable limits. Comparison of the marginal gap values of shoulder and chamfer finish lines it was observed that shoulder finish lines showed more appropriate values in the HIP group (SHO/HIP 35, 8µm) whereas chamfer finish line showed more appropriate values in the NON-HIP group (CHA / NHIP 60, 2µm). In our opinion, these differences between the two types of finish lines might result from material differences or the difference of reading parts of CAD-CAM systems. Repeatability is one of the most critical pre-conditions in appropriate measurement of the marginal gap [35]. In the present study; in order to start measuring from the same point of each specimen, guiding points were described (MB, B, DB, ML, L and DL) and marked across of the entire circumference of stainless steel specimens. According to the literature, for the studies focusing on marginal gap measurements, five to twelve specimens were used for each group [36]. We have used ten specimens for each group in our study. It has been proclaimed that, one of the most important parameters is the standard deviation of measured marginal gap and an acceptable standard deviation is thought to be approximately 20µm [15,18,22,37]. In the current study, standard deviation values were calculated from 13, 5µm to 35, 85µm. Especially 35, 85µm standard deviation value was obtained on the partially sintered bevel finish line group. The reason of this value could be attributed to the undulated shrinkage during sintering of blocks with porous structure.

Conclusion

The marginal gap of frameworks obtained from fully sintered zirconia blocks was smaller than the marginal gap of frameworks obtained from partially sintered zirconia blocks. The amount of marginal gap at zirconium frameworks has been affected by the type of finish line. The amount of marginal gap of shoulder and chamfer type finish lines presented with smaller gaps than the bevel type finish line. Average values of six experimental groups were found under 120µm, which were all within clinically acceptable limits. Further investigations are necessary in this field, even if the quality of marginal fit depends on the CAD/ CAM system used.

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